Categorization in Mechanically Ventilated Pediatric Subjects: A Proposed Method to Improve Quality

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Categorization in Mechanically Ventilated Pediatric Subjects: A Proposed Method to Improve Quality

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BACKGROUND: Thousands of children require mechanical ventilation each year. Although mechanical ventilation is lifesaving, it is also associated with adverse events if not properly managed. The systematic implementation of evidence-based practice through the use of guidelines and protocols has been shown to mitigate risk, yet variation in care remains prevalent. Advances in health-care technology provided the ability to stream data about mechanical ventilation and therapeutic response. Through these advances, a computer system was developed to enable the coupling of physiologic and ventilation data for real-time interpretation. Our aim was to assess the feasibility and utility of a newly developed patient categorization and scoring system to objectively measure compliance with standards of care. METHODS: We retrospectively categorized the ventilation and oxygenation statuses of subjects within our pediatric ICU utilizing 15 rules-based algorithms. Targets were predetermined based on generally accepted practices. All patient categories were calculated and presented as a percent score (0–100%) of acceptable ventilation, acceptable oxygenation, barotrauma-free, and volutrauma-free states. RESULTS: Two hundred twenty-two subjects were identified and analyzed encompassing 1,578 d of mechanical ventilation. Median age was 3 y, median ideal body weight was 14.7 kg, and 63% were male. The median acceptable ventilation score was 84.6%, and the median acceptable oxygenation score was 70.1% (100% being maximally acceptable). Potential for ventilator-induced lung injury was broken into 2 components: barotrauma and volutrauma. There was very little potential for barotrauma, with a median barotrauma-free state of 100%. Median potential for a volutrauma-free state was 56.1%. CONCLUSIONS: We demonstrate the first patient categorization system utilizing a coordinated data-banking system and analytics to determine patient status and a surveillance of mechanical ventilation quality. Further research is needed to determine whether interventions such as visual display of variance from goal and patient categorization summaries can improve outcomes. (ClinicalTrials.gov registration NCT02184208.) Key words: computer decision support; mechanical ventilation; ventilator-induced lung injury; quality; protocols; evidence-based practice; data. [Respir Care 2016;61(9):1168–1178. © 2016 Daedalus Enterprises]

Introduction

Hospitals are facing increasing pressure to improve outcomes and lower costs. The ICU, where the most critical and costly care is provided to the sickest patients, represents an opportunity to address both patient-specific outcomes and reduction in costs. The ICU is a complex environment where lifesaving technology, such as mechanical ventilation, is administered. By capturing and analyzing data generated in this environment, clinicians may stream-
line and optimize care for individual patients. Individualized treatment plans based on patient continuous data can augment clinical decision-making and potentially improve outcomes.

Of the critically ill patients in the ICU, an estimated 30–50% require some type of ventilatory support. Respiratory disorders are the main cause of respiratory failure in children. Although mechanical ventilation is generally lifesaving, it can be associated with adverse events if not appropriately initiated, maintained, and monitored. The systematic implementation of evidence-based practice through the use of guidelines and protocols has been shown to mitigate the risk, yet variation in care among and within institutions remains prevalent. Variation in the application of mechanical ventilation therapy may pose a significant health risk to patients by prolonging duration of ventilation and length of hospital stay and may increase the likelihood of adverse events.

When not guided by evidence-based guidelines, clinical decisions about mechanical ventilation rely heavily on intermittent manual assessments and clinical judgment often without consideration of continuously monitored pulmonary mechanics, gas exchange, and cardiopulmonary interactions or trends. Most approaches to mechanical ventilation are standardized; however, implementation and timely execution of mechanical ventilation requires knowledge and concern regarding lung protection and overall patient safety.

Mechanical ventilation has undergone significant advances over the last decade as a result of improved monitoring, more established predictors for titrating support, and better understanding of how lung injury occurs. There is evidence that adopting clinical practice guidelines together with lung-protective ventilation strategies reduces mortality in adult patients. Quality of mechanical ventilation should focus on reducing the duration of mechanical ventilation, stay, and cost of care by monitoring goal attainment during mechanical ventilation, identifying practice variance, and liberating patients as soon as the reasons for mechanical ventilation are resolved. In an effort to assist clinicians with determining their performance, we developed a system of care called computer-aided mechanical ventilation to leverage these data to determine the quality of mechanical ventilation care. A computerized method of patient status identification from continuous data is presented.

**Methods**

Following institutional review board approval and registration with ClinicalTrials.gov, we retrospectively analyzed subjects who required invasive mechanical ventilation within our 2 pediatric ICUs (30-bed medical/surgical ICU and 29-bed cardiac ICU). Due to the pilot nature of this study, we began a phase rollout of collecting data on mechanically ventilated patients who were anticipated to be ventilated for >3 h. Subjects were prospectively selected by 2 respiratory therapists in charge of the limited rollout in May of 2013. Data recording was based on the availability of connectivity equipment to a data network that stores, analyzes, and displays information dubbed the T3 (Etiometry, Boston, Massachusetts) system.

**Inclusion Criteria for Data Analysis**

Subjects were included through a sampling of mechanical ventilation data found within the T3 analytics platform for >3 h within our T3 analytics platform.
Exclusion Criteria for Data Analysis

Patients were excluded for 4 reasons: (1) if the system was unavailable; (2) if the ventilator data output was not compatible with our system; (3) if the medical record number or name was not found within our electronic medical record; or (4) if alternative modes of ventilation, such as high-frequency oscillatory ventilation or airway pressure release ventilation, were used.

Data Collection and Display System

This was a prospective deployment followed by a retrospective analysis pilot study designed to demonstrate the feasibility of the system and identify strengths and weakness of the T3 data collection and analytics platform developed by the Departments of Anesthesia and Cardiology at Boston Children’s Hospital. The primary functions of the T3 system are to aggregate, store, and display comprehensive real-time patient data for clinicians. The technology provides a platform to track patient data on a single, easy-to-manipulate monitoring system, viewable on standard web browsers within the hospital infrastructure. Additional functionality includes the ability to formulate and collate multivariable algorithms for research purposes. It is this analytics platform that we evaluated.

Data Handling

The computer-aided mechanical ventilation module was built upon a web-based platform for data collection developed to streamline physiologic and mechanical ventilation data collection and continuously display these data. In brief, the T3 system utilizes an FDA-cleared data collection system previously used for research endeavors.

Mechanical ventilators stream their data to our critical care bedside monitors (MP90 or MX800, Philips Healthcare, Amsterdam, Netherlands) through a proprietary data connectivity engine by the same company labeled Intellibridge, utilizing the EC-10 module and brand-specific cables. The T3 system uses the medical record number as the key identifier to request and obtain the patient’s name, date of birth, and sex from the admission, discharge, transfer server all within our secure intranet infrastructure. There is one T3 server for each ICU. Nightly, the T3 ICU servers export data to a research database to allow future analysis.

The physiologic and mechanical ventilation data were combined manually with demographics and reason for mechanical ventilation from the respiratory therapy quality improvement database. The 80 reasons for mechanical ventilation were grouped into 4 general cohorts: medical, surgical, cardiac surgery, and cardiac. Ideal body weight was extracted from the electronic medical record. If data utilized in the calculation of an algorithm were not available, no categorization would be displayed. See Figure 1 for data flow from the multiple sources.

Subject Categorization

A novel method for categorizing the state of a patient undergoing mechanical ventilation summarizing a patient’s condition was developed to mimic how clinicians analyze data at the bedside. Fifteen rules-based algorithms were developed that cover 3 domains: (1) ventilation, (2) oxygenation, and (3) ventilator-induced lung injury. This process involves receiving, selecting, retrieving, and categorization. Table 1 provides the details of the rules-based algorithms. The goal of subject categorization was to convey information about the subject’s status from predetermined generally accepted goals of mechanical ventilation. All subject categorization is presented in percent of recorded time and chosen before analysis. None of the subject categorization was made available in real time to clinicians.

Categorization of Ventilation and Oxygenation

Categorization of ventilation and oxygenation are detailed according to generally accepted goals of mechanical ventilation within traditional definitions. Inputs such as clinical practice guidelines, standards of care, and policies provide the intent and goals of mechanical ventilation. When clinical knowledge is paired with the clinically relevant continuously available data, it is sent to the algorithms segment to be explored. Within the algorithms...
segment, previously validated data-driven algorithms were used to develop the patient categorization. Within the algorithm aggregator, the algorithms were applied to the continuous data to describe a subjects’ status. Figure 2 describes how clinical knowledge paired with clinical data was leveraged to fulfill the algorithm development and implementation. The goal of this computerized method of assessment is to determine how well goals of mechanical ventilation are achieved without contributing to settings associated with ventilator-induced lung injury. Severe categories of ventilation are triggered by the cardiopulmonary interactions of abnormal ventilation. In the absence of abnormal ventilation triggers, the acceptable ventilation category was assumed. Heart rate was chosen, because it is

### Table 1. The 3 Domains, 15 Categories, and Rules-Based Algorithms

<table>
<thead>
<tr>
<th>Domains and Categories</th>
<th>Definition</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>Ventilation</strong></td>
<td></td>
</tr>
<tr>
<td>Acceptable ventilation score</td>
<td>All ventilation goals achieved</td>
</tr>
</tbody>
</table>
| Tachypnea              | ≤6 mo: \( f > 55 \text{ breaths/min} \); heart rate < 160 beats/min  
3 to <6 y: \( f > 45 \text{ breaths/min} \); heart rate < 140 beats/min  
>6 y: \( f > 30 \text{ breaths/min} \); heart rate < 90 beats/min |
| Severe tachypnea        | <6 mo: \( f > 55 \text{ breaths/min} \); heart rate > 160 beats/min  
7 mo to <3 y: \( f > 45 \text{ breaths/min} \); heart rate > 140 beats/min  
3 to <6 y: \( f > 40 \text{ breaths/min} \); heart rate > 110 beats/min  
>6 y: \( f > 30 \text{ breaths/min} \); heart rate > 90 beats/min |
| Insufficient ventilation | ≤6 mo: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); \( f > 55 \text{ breaths/min} \); heart rate > 160 beats/min  
7 mo to <3 y: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); \( f > 45 \text{ breaths/min} \); heart rate > 140 beats/min  
3 to <6 y: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); \( f > 40 \text{ breaths/min} \); heart rate > 110 beats/min  
>6 y: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); \( f > 30 \text{ breaths/min} \); heart rate > 90 beats/min |
| Hypoventilation         | ≤6 mo: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); heart rate < 160 beats/min  
7 mo to <3 y: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); heart rate < 140 beats/min  
3 to <6 y: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); heart rate < 110 beats/min  
>6 y: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); heart rate < 90 beats/min |
| Severe hypoventilation  | ≤6 mo: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); heart rate > 160 beats/min  
7 mo to <3 y: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); heart rate > 140 beats/min  
3 to <6 y: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); heart rate > 110 beats/min  
>6 y: \( P_{E\text{TCO}_2} > 55 \text{ mm Hg} \); heart rate > 90 beats/min |
| Hyperventilation        | ≤6 mo: \( P_{E\text{TCO}_2} < 35 \text{ mm Hg} \); heart rate < 160 beats/min  
7 mo to <3 y: \( P_{E\text{TCO}_2} < 35 \text{ mm Hg} \); heart rate < 140 beats/min  
3 to <6 y: \( P_{E\text{TCO}_2} < 35 \text{ mm Hg} \); heart rate < 110 beats/min  
>6 y: \( P_{E\text{TCO}_2} < 35 \text{ mm Hg} \); heart rate < 90 beats/min |
| Severe hyperventilation | ≤6 mo: \( P_{E\text{TCO}_2} < 35 \text{ mm Hg} \); heart rate > 160 beats/min  
7 mo to <3 y: \( P_{E\text{TCO}_2} < 35 \text{ mm Hg} \); heart rate > 140 beats/min  
3 to <6 y: \( P_{E\text{TCO}_2} < 35 \text{ mm Hg} \); heart rate > 110 beats/min  
>6 y: \( P_{E\text{TCO}_2} < 35 \text{ mm Hg} \); heart rate > 90 beats/min |
| **Oxygenation**         |            |
| Acceptable oxygenation score | S/F ≥264; <328; >452 |
| Mild hypoxia            | S/F ≥221; <264 |
| Moderate hypoxia        | S/F ≥153; <221 |
| Severe hypoxia          | S/F <153 |
| Hyperoxia               | S/F ≥328; ≤452 |
| **VILI**                |            |
| Barotrauma-free         | PIP ≤30 |
| Volutrauma-free         | Exhaled tidal volume >4 mL/kg IBW; <8 mL/kg IBW |

Units of measure for all categories were percentage of time.  
\( f \) = breathing frequency  
\( P_{E\text{TCO}_2} \) = end-tidal carbon dioxide pressure  
S/F = \( S_{\text{O}_2}/F_{\text{IO}_2} \)  
VILI = ventilator-induced lung injury  
PIP = peak inspiratory pressure  
IBW = ideal body weight
continuously available and an indication of hemodynamic effects of the given ventilator strategy. Heart rate was only evaluated after an abnormal ventilation trigger, such as high or low end-tidal carbon dioxide pressure ($P_{ETCO_2}$ or breathing frequency). See Table 1 for the definition of each condition.

Oxygenation categories are designed to utilize the $SpO_2/FIO_2$ in an attempt to add context to $SpO_2$ measurement alone, as reported previously by the Pediatric Acute Lung Injury Consensus recommendations and validated by Tripathi et al. Like heart rate, $SpO_2$ and $FIO_2$ are continuously available as the standard of care. In the absence of abnormal oxygenation triggers, the acceptable oxygenation category was assumed. See Table 1 for the breakdown of each oxygenation-related condition. Note that hyperoxia is excluded from negatively affecting the acceptable oxygenation category.

Data/Statistical Analysis

Data were collected from the mechanical ventilator and physiologic monitors every 5 s. A median 1-min filter from the 12 data points/min was applied. According to Levene’s test of homoscedasticity, the data are not normally distributed; therefore, we have provided medians and 25–75% interquartile range calculated from the sampled parameters according to the absolute number of measurements. JMP 12.0 (SAS Institute, Cary, North Carolina) was utilized for the statistics, categorization, and graphs. One-way analysis of variance using the nonparametric Kruskal-Wallis test was performed to determine significance. Comparison of pairs was performed utilizing the nonparametric Wilcoxon method of analysis. $P$ values of $<.05$ were considered significant.

Calculations

The oxygen saturation index was developed by Thomas et al. to noninvasively assess acute lung disease and was calculated within this cohort. Although we chose to use $SpO_2/FIO_2$ to categorize mild, moderate, or severe hypoxia, we could have easily chosen the oxygen saturation index.

Results

Subject Characteristics

Two hundred twenty-two subjects (20% of patients receiving mechanical ventilation) were enrolled and analyzed encompassing 1,578 d of mechanical ventilation from May 8, 2013 to October 31, 2015. The median (interquartile range) age was 3 (0.7–12.3) y, median ideal body weight was 14.7 (7.2–35) kg, and 63% of the subjects were male. See Table 2 for additional demographics by cohort. Age and weight were significantly different among groups.

Our goal was to develop a system that could obtain data from multiple devices, therefore not being device-specific. This was achieved with the exception of 2 devices. Subjects ($n = 44$) were excluded from either the ventilation or
oxygenation assessments because either $P_{ETCO_2}$ or $FIO_2$ data were missing. We isolated this missing data to the CareFusion Avea ($P_{ETCO_2}$) and Philips V60 and Philips NM3 ($P_{ETCO_2}$ and $FIO_2$). Due to a driver software conflict between Philips and CareFusion, $P_{ETCO_2}$, although measured and displayed, was not provided in the Health Level 7 data feed. Therefore, ventilation categorization could not be performed in these subjects ($n = 40$), but oxygenation categorization could be performed. The Philips V60 does not measure $FIO_2$ or $P_{ETCO_2}$; therefore, no oxygenation or ventilation categorization could be performed ($n = 2$). The Philips NM3 measures all parameters except for $FIO_2$. No oxygenation categorization was provided in those subjects ($n = 2$).

Ventilation Categories

The median (interquartile range) acceptable ventilation score was 84.6% (69.4–95.3%) for the entire cohort. Acceptable ventilation was not significantly different among the surgical, medical, and cardiac cohorts; however, there was a significant difference between the cardiac surgery and general surgery groups ($P = .03$). See Table 3 for details. Figure 3 describes the 6 abnormal ventilation categories organized by cohort.

Oxygenation Categories

The median (interquartile range) acceptable oxygenation score was 70.1% (27.2–95.3%) among all mechanically ventilated subjects. There were no significant differences among cohorts. See Table 3 for details. Figure 4 describes the 4 categories of abnormal oxygenation organized by cohort.

Heart Rate, Respiratory Rate, and Ventilation Index

Heart rate, breathing frequency, spontaneous breathing frequency, and modified ventilation index are presented in 4 age subcategories and by reasons for mechanical ventilation (see Table 4). All data are presented as medians and interquartile ranges.

Table 2. Demographics, Parameters of Oxygenation, Ventilation, Pressures, and Recording Time Parameters That Are Not Age-Dependent

<table>
<thead>
<tr>
<th>Parameters</th>
<th>Surgical</th>
<th>Medical</th>
<th>Cardiac Surgery</th>
<th>Cardiac</th>
<th>$P$</th>
</tr>
</thead>
<tbody>
<tr>
<td>Demographics</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Age, y</td>
<td>3 (0.85–13)</td>
<td>5 (1.1–12.5)</td>
<td>0.11 (0.01–4.5)</td>
<td>0.7 (0.11–13)</td>
<td>.02</td>
</tr>
<tr>
<td>Weight, kg</td>
<td>14.7 (7.1–36)</td>
<td>17.5 (9.3–36.7)</td>
<td>5.6 (3.2–18.9)</td>
<td>7 (5.3–55)</td>
<td>.01</td>
</tr>
<tr>
<td>$n$</td>
<td>113</td>
<td>84</td>
<td>22</td>
<td>3</td>
<td></td>
</tr>
</tbody>
</table>

| Oxygenation                          |                |               |                 |              |      |
| $S_{AO_2}$, %                        | 98.6 (97.9–99.2)| 98.3 (97.2–99.2)| 98.8 (90.3–99.7)| 98.1 (80.8–99.1)| .30  |
| $F_{IO_2}$, %                        | 36.3 (31.2–41.8)| 37.6 (31.6–44)| 40.1 (31.2–40.8) | 37.8 (37.5–43.5)| .53  |
| $S/F$                                | 286 (243–326)  | 279 (231–326)  | 248 (231–298)   | 266 (190–270) | .14  |
| OSI                                  | 3.2 (2.6–4.2)  | 3.8 (2.9–4.8)  | 3.5 (2.8–4.2)   | 4.5 (3.3–6.1) | .064 |

| Ventilation                          |                |               |                 |              |      |
| $P_{ETCO_2}$, mm Hg                  | 42.9 (40.4–46.7)| 41.9 (37.7–45.5)| 34 (29.8–46)    | 44.9 (44.9–45)| .01  |
| $V_t/kg                              | 7 (5.8–8)      | 7.3 (6.1–8.3)  | 8 (6.8–9)       | 7.3 (5.6–7.5)| .064 |

| Pressures                            |                |               |                 |              |      |
| $PIP$, cm H$_2$O                      | 18.1 (15.4–21.3)| 19.3 (15.8–22.1)| 19.6 (18.5–22.9)| 23.9 (19.9–26)| .058 |
| PEEP, cm H$_2$O                       | 5 (4.9–5.9)    | 5.9 (5–7.1)    | 5 (4–5)         | 5.1 (5–6.6)  | <.001|

| Time                                 |                |               |                 |              |      |
| Recording time, d                    | 2.7 (1–9.3)    | 4.9 (1.6–10)  | 1.8 (0.2–5.6)   | 12 (6.9–15.8)| .08  |
| Percentage recording of duration of mechanical ventilation, % | 35 | 62 | 40 | 100 |      |

Data are median (interquartile range). $P$ values are according to the Kruskal-Wallis method.

$S/F = S_{AO_2}/F_{IO_2}$

OSI = oxygen saturation index

$P_{ETCO_2}$ = end-tidal carbon dioxide pressure

$PIP$ = peak inspiratory pressure

$V_t$ = tidal volume
The modified ventilation index was significantly higher in the surgical cohort when compared with the medical cohort ($P = .003$).

**Ventilator-Induced Lung Injury**

Ventilator-induced lung injury parameters were broken down into 2 categories, barotrauma-free and volutrauma-free states. Median (interquartile range) percentage of recorded time spent in a potential barotrauma-free state was 100% (99.9–100%) among all mechanical ventilation subjects. There were no significant differences among cohorts of subjects. The median (interquartile range) percentage of recorded time spent in a potential volutrauma-free state was 56.1% (24.8–87.6%) among all mechanical ventilation subjects.
Discussions

To our knowledge, this is the first description in the literature of the utility and application of a patient categorization system employing multiple sources of data to be used as a benchmark for future quality improvement interventions. Our findings represent an objective measure of opportunities within our own practice to discuss and potentially implement solutions for better quality patient care. Our hope is that positive trends in goal attainment (control) will lead to improved outcomes or that negative trends in goal attainment (lack of control) will serve as an early warning system before a negative patient outcome occurs.

Goals of Mechanical Ventilation

The quality of mechanical ventilation is often based on outcomes such as length of stay, time to liberation, ventilator-free days, ventilator-associated pneumonia, incidences of pneumothoraces, or brain or airway injury, yet these quality measures are end results or retrospective in nature. Although certainly not exhaustive, our effort was to capture generally accepted goals of mechanical ventilation while attempting to be as lung-protective as possible based on current evidence. Often, set goals of mechanical ventilation are ideal but not real, meaning that we have great intentions but rarely measure how well we meet those intentions. Measuring the impact of these goals on mechanical ventilation outcomes can be challenging. When clinicians find patients outside of the goals, they often correct the situation without any context for the length of time the patient may have been outside of the goal. Due to alarm fatigue, we often set our alarms or alerts broadly so as to only notify clinicians of life-altering events. The goal of 100% compliance may not be obtainable as certain situations are outside of the clinician’s control. However, leveraging a computerized
system to identify outliers to the standard of care will improve our MV quality.

**Limitations**

We were not able to obtain complete recordings of every mechanically ventilated patient in our 2 ICUs because the number of devices (Intellibridge EC10) limited our ability to capture these data. Therefore, we were not able to draw outcome conclusions based on our patient categorization and instead report our findings as percentage of recorded time. Since the beginning of our study, we have purchased enough devices to connect every ventilator and will be able to report clinical outcomes in the near future.

**Disease-Specific Goals**

Although we did not develop disease- or patient-specific goals of mechanical ventilation, this clearly needs to be the next step in our program’s progression. We set out to determine the feasibility of our system of care by utilizing broad goals that are applicable to the majority of our patients receiving mechanical ventilation. One limitation of not setting disease- or patient-specific goals is the fact they may actually disguise the best care. For example, to provide neuro-protective ventilation, one may target a \( P_{ETCO_2} \) of 30–40 mm Hg to ensure a normal \( P_{aCO_2} \) of 35–45 mm Hg, or in a patient with severe pediatric ARDS, a tidal volume of 3–6 mL/kg may be the more appropriate target. However, because the purpose of the presented investigation was to set and monitor boundaries in which the majority of patients should be maintained, this provides an adequate system.

**Oxygenation Categories**

The oxygenation categories are an area in which there is much debate. The majority of pediatric patients are placed on mechanical ventilation for hypoxic respiratory failure, so it is not surprising that mild hypoxemia is a common occurrence. Some even employ a strategy of permissive hypoxemia to avoid lung injury. Normal gas exchange should be a goal of mechanical ventilation except when attempting to achieve normal gas exchange violates lung-protective strategies. Normal gas exchange should be secondary to \( F_{O_2} \), tidal volume, and pressure limits.

**Intraoperability**

There are several limitations to this method that we have discovered along the way. One is the ability to capture all of the data from devices within our ICU. Not all devices provide data in the same language which has limited our ability analyze. As mentioned, we had to exclude some patient categorizations due to the lack of available data. We narrowed this down to a Philips driver and CareFusion ventilator software compatibility issue, which we were unable to resolve.

**Labeling of Parameters**

Health Level 7 is a set of international standards for the transfer of clinical and administrative data between soft-

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**Table 4. Results by Age Category and Cohort**

<table>
<thead>
<tr>
<th>Parameters and Subgroups</th>
<th>Surgical</th>
<th>Medical</th>
<th>Cardiac Surgery</th>
<th>Cardiac</th>
<th>( P )</th>
</tr>
</thead>
<tbody>
<tr>
<td>Heart rate beats/min</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>≤6 mo</td>
<td>127.6 (114.3–132.8)*</td>
<td>122.2 (114.3–132.8)</td>
<td>147.1 (133.9–158)*</td>
<td>147</td>
<td>.01</td>
</tr>
<tr>
<td>7 mo to &lt;3 y</td>
<td>111.4 (22.56, 12)</td>
<td>116.5 (16.5, 19)</td>
<td>145.2 (14.7, 7)</td>
<td>100 (-, 1)</td>
<td>.08</td>
</tr>
<tr>
<td>&gt;3 to ≤6 y</td>
<td>110 (96.9–123)</td>
<td>113.4 (108.2–124.2)</td>
<td>ND</td>
<td>ND</td>
<td>.40</td>
</tr>
<tr>
<td>&gt;6 y</td>
<td>95.1 (77.5–107.3)</td>
<td>102 (90.6–119.2)*</td>
<td>67 (61.5–85)*</td>
<td>108.1</td>
<td>.006</td>
</tr>
<tr>
<td>Breathing frequency beats/min</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>≤6 mo</td>
<td>40.4 (23.5–48.9)*</td>
<td>25.2 (21.3–32.5)*</td>
<td>25.2 (23.4–32.5)</td>
<td>24.8</td>
<td>.031</td>
</tr>
<tr>
<td>&gt;7 mo to ≤3 y</td>
<td>24 (21.5–27.5)*</td>
<td>21.3 (20.8–22.6)*</td>
<td>22.2</td>
<td>27.8</td>
<td>.01</td>
</tr>
<tr>
<td>&gt;3 to ≤6 y</td>
<td>23 (20.1–25.3)</td>
<td>20.7 (16.3–23.4)</td>
<td>ND</td>
<td>ND</td>
<td>.13</td>
</tr>
<tr>
<td>&gt;6 y</td>
<td>15.5 (13.5–19.1)</td>
<td>16.2 (14–22)</td>
<td>15.6 (12–16)</td>
<td>21.2</td>
<td>.32</td>
</tr>
<tr>
<td>Spontaneous breathing frequency beats/min</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>≤6 mo</td>
<td>27.4 (15.2–44)</td>
<td>20.2 (14.3–25.2)</td>
<td>24.5 (15.9–32.5)</td>
<td>20.1</td>
<td>.36</td>
</tr>
<tr>
<td>&gt;7 mo to ≤3 y</td>
<td>17.4 (9.9–22.4)</td>
<td>15 (8.4–20.6)</td>
<td>17.9</td>
<td>25</td>
<td>.35</td>
</tr>
<tr>
<td>&gt;3 to ≤6 y</td>
<td>14.1 (12.5–19.5)</td>
<td>11.1 (7.6–18.8)</td>
<td>ND</td>
<td>ND</td>
<td>.35</td>
</tr>
<tr>
<td>≥6 y</td>
<td>12.1 (7.7–17.5)</td>
<td>13.5 (8.7–19.6)</td>
<td>10 (4.8–15.3)</td>
<td>10.9</td>
<td>.46</td>
</tr>
</tbody>
</table>

Data are median (interquartile range). \( P \) values are according to the Kruskal-Wallis method. * \( P \) value comparisons using Wilcoxon method.
ware applications. Although this standardized way of communicating is helpful at moving large amounts of data in an efficient way, there are no universal definitions of parameters within health care. For example, one ventilator can send out data in Health Level 7 format and label it PIP for peak inspiratory pressure, and another ventilator can send out the same parameter but label it PAW for peak airway pressure, making it difficult to find, capture, or track these parameters within a large database. This requires a manual process to monitor, particularly when utilizing different ventilators or monitors. We have created a code library for each of the ventilators within our institution and will create a program to align like parameters in the near future to resolve and ensure data integrity.

Severe Categories

Historically, severe categories were often based on how far a value was above or below the given monitored parameter. Some would use SD values to determine this range of high (or low) to severely high (or low). However, when critically thinking of how most clinicians obtain and analyze data, they often look for relationships within multiple organ systems. One relationship that most focus on is cardiopulmonary interaction. We have a term in pediatrics of “comfortably tachypneic.” This means that the patient is breathing fast, but no other organ systems are showing signs or symptoms of distress. In today’s electronic world, we can come closer and closer to being able to retrieve and analyze data similar to the best clinician within a given practice. This may allow future utilization of expert opinion on a minute by minute basis.

Conclusions

We demonstrate the first patient categorization system that utilizes multiple data sources and calculations to determine a patient status and indicator of mechanical ventilation quality. Further research is needed to determine whether interventions such as visual display of variance from goal and patient categorization summaries can improve patient outcomes by providing clinicians with useful and objective information.

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